

IMMERSED BOUNDARY METHODS FOR DNS OF GAS-SOLID FLOWS

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Training School “*Behaviour of Non-Spherical Particles in Flows*”
COST FP1005

1 INTRODUCTION

- ALE formulation
- Immersed Boundary Method

2 ISSUES WITH IBM - MOVING BODIES

3 IMPROVEMENTS FOR IBM

- Fresh/dead cell treatment
- Mirroring interpolation
- Continuity equation modifications
- Cell merging

4 RESULTS

- Oscillating sphere
- Sedimenting sphere

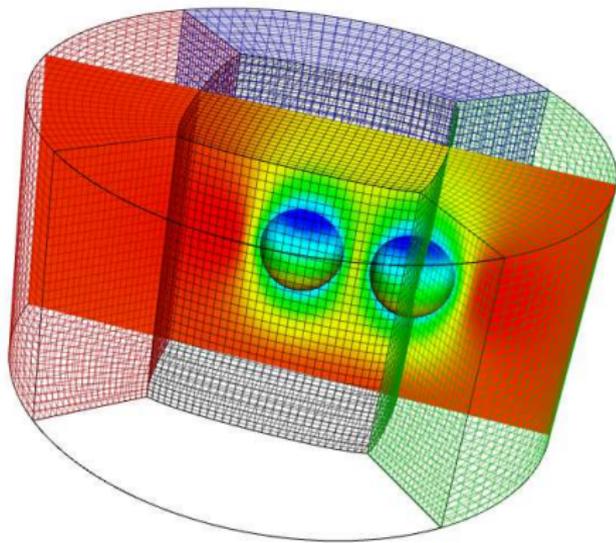
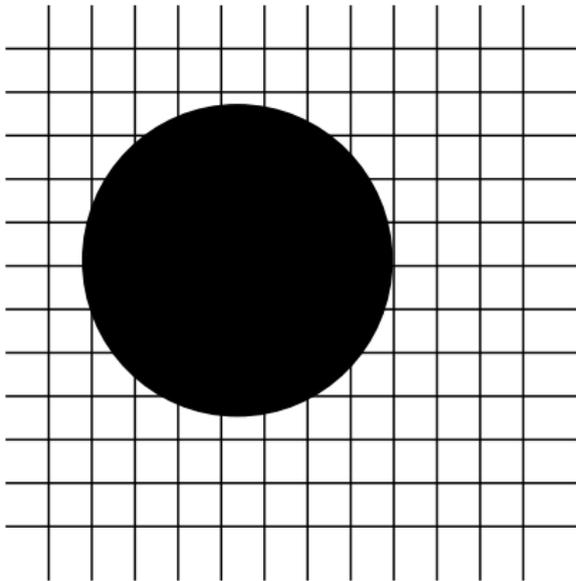
5 PARTICLE-PARTICLE INTERACTIONS

- Methods required to calculate interaction of multiple particles
- Results of the interaction of multiple particles

6 APPLICATION TO NON-SPHERICAL PARTICLES

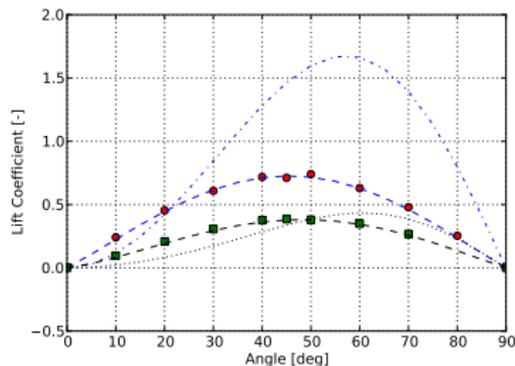
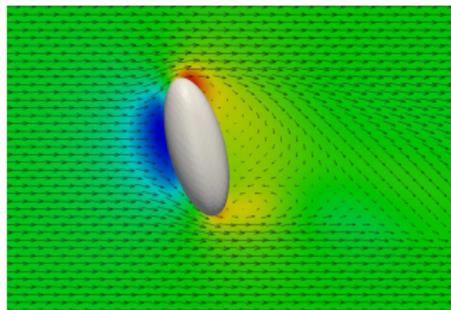
- Drag, Lift and Torques

DNS METHODS FOR PARTICLES

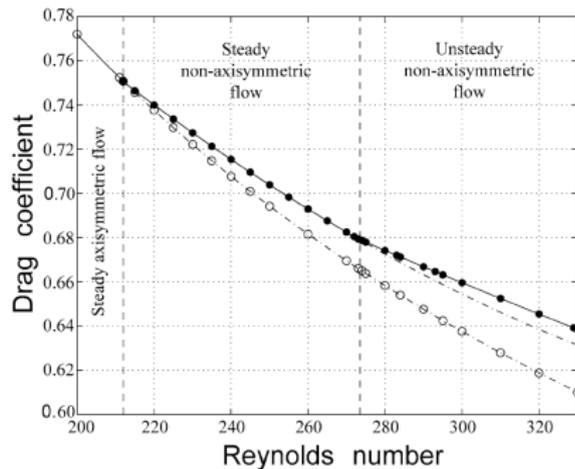
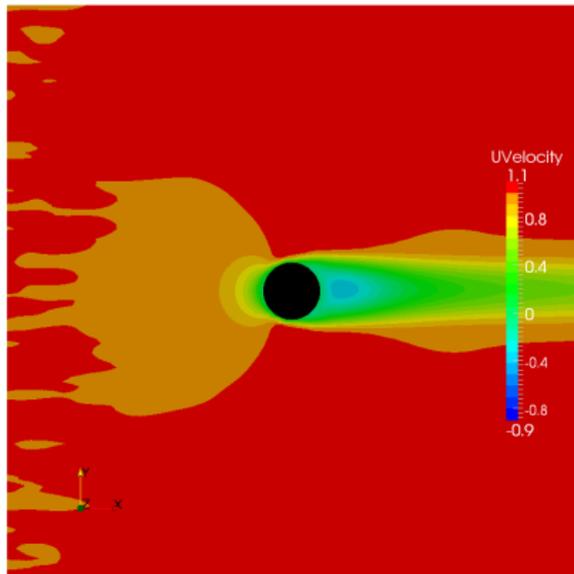


MOTIVATION FOR DNS

- Accurate flow solution
- Physical insight
 - Flow transition
 - Vortex structures
 - Accurate forces
- Too detailed to be “practical”
 - Can be used to derive engineering models for large scale simulations

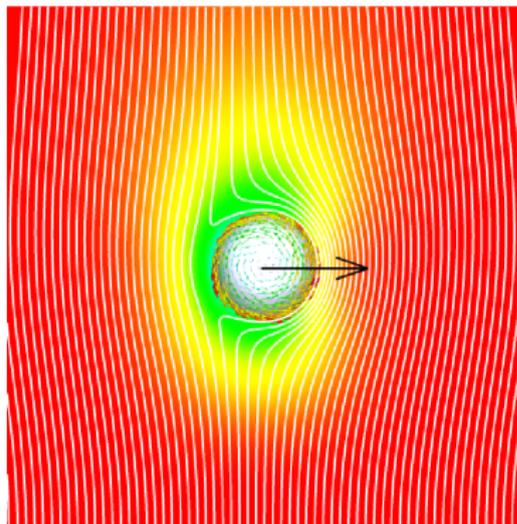
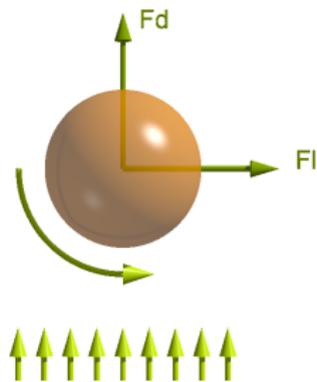


“TRUE” DNS METHODS

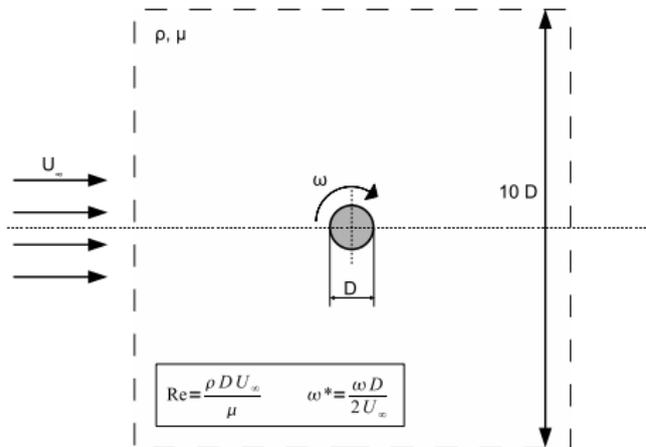


ROTATING SPHERE

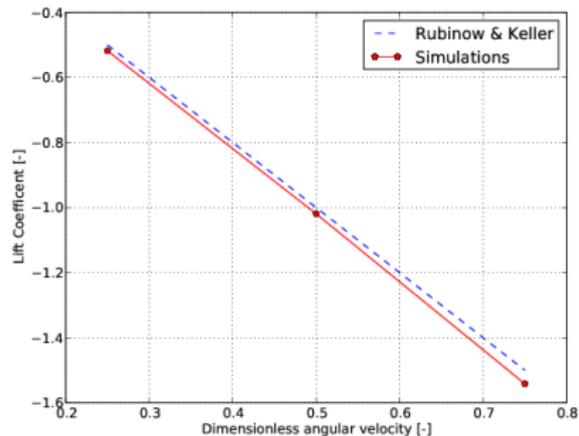
Velocity Field and Streamlines



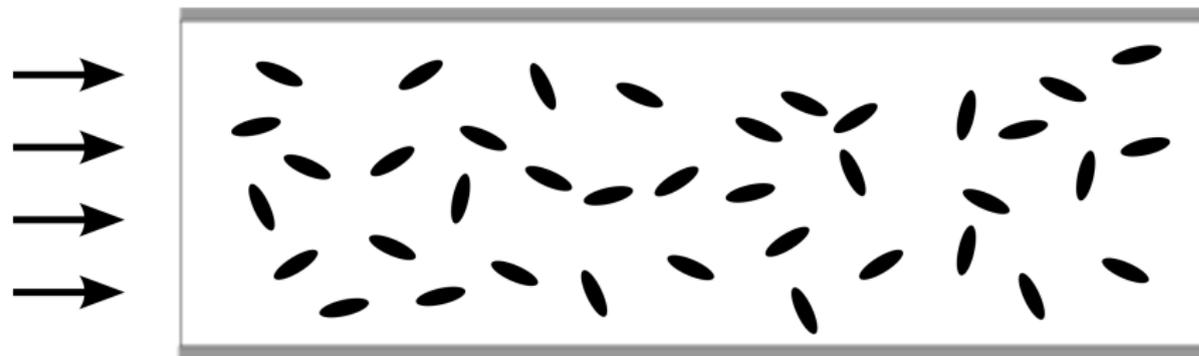
ROTATING SPHERE



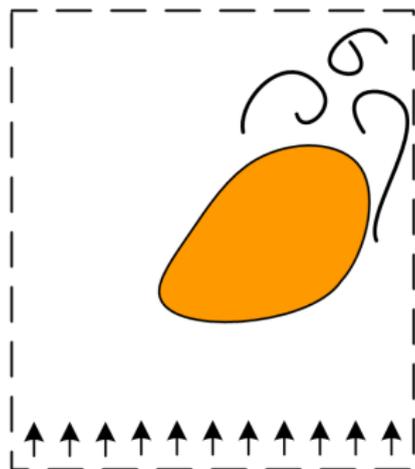
$Re_D < 1$, Rubinov & Keller (1961)



EXAMPLE APPLICATION - CHANNEL FLOW WITH PARTICLES



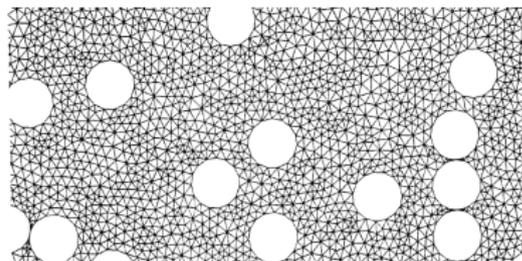
- Channel flow with non-spherical particles ($Re = 42'000$)
- Use DNS to model the forces on particles: $F_P = f(Re, \varphi)$
- Solve the problem using LES and point-particle approach



Strategies:

- Body fitting meshes (ALE formulation)
 - Particles are meshed
 - Accurate but expensive
 - Re-meshing required
 - Good when little movement is required.
- Alternative methods
 - Immersed Boundary
 - Cartesian Grid
 - Fictitious Domain
 - Lattice Boltzmann

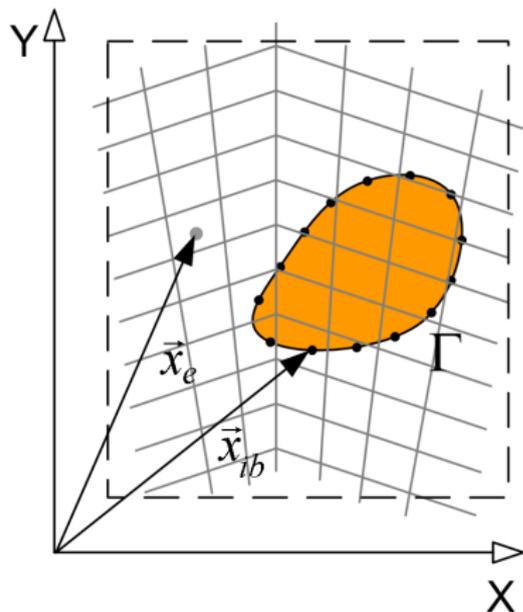
ARBITRARY LAGRANGIAN EULERIAN (ALE)



Hu (1996)

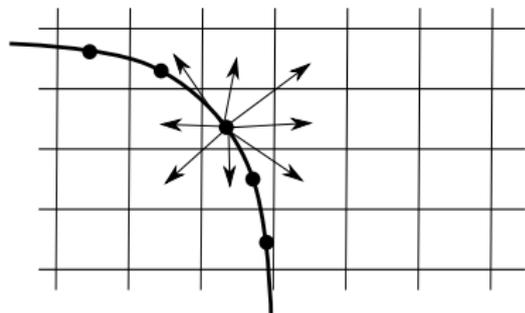
- The Lagrangian particles are meshed.
- Very accurate.
- Very expensive, difficult to have accurate interpolation.
- Remeshing required.
- Good for problems where little movement is required.

IMMERSED BOUNDARY METHOD



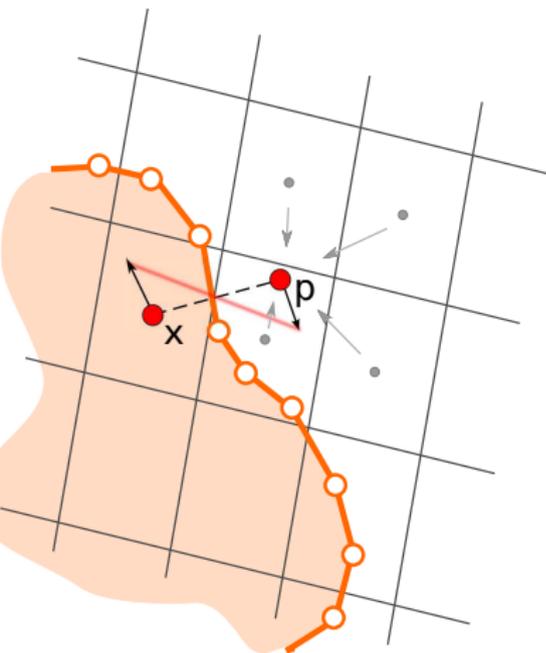
- Fluid domain is represented by an Eulerian grid
- A Lagrangian grid represents the solid-fluid interface
- Presented approach:
 - No-slip velocity boundary condition on the surface
 - Zero gradient pressure boundary condition on the surface
 - Force calculated from the resolved flow field

DISTRIBUTED IMMERSED BOUNDARY METHOD



- “Classic” IBM methods are distributed.
- A force is determined in the Lagrangian control points, so the fluid velocity matches the control point velocity.
- This force is distributed along the Eulerian neighbours of the control point.

MIRRORING PRINCIPLE



Mark and van Wachem, JCP 207, 2008

- Project (x) into the fluid domain to create p
- Internal point velocity is set to satisfy the no-slip boundary condition at the surface

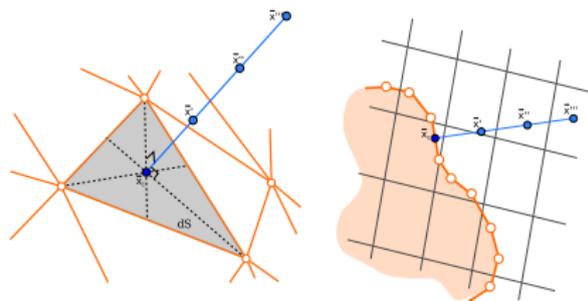
$$u_{IB}^i = \frac{1}{2} (u_{IN}^i + \sum \beta_m u_m^i)$$

- Internal point pressure is set to obtain zero pressure gradient at the surface

$$(p_{IN}^i - \sum \beta_m p_m^i) = 0$$

- Coefficients β_m from geometric interpolation function.

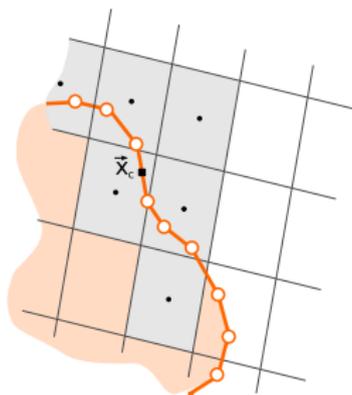
FORCE CALCULATION



Force obtained from the resolved flow field:

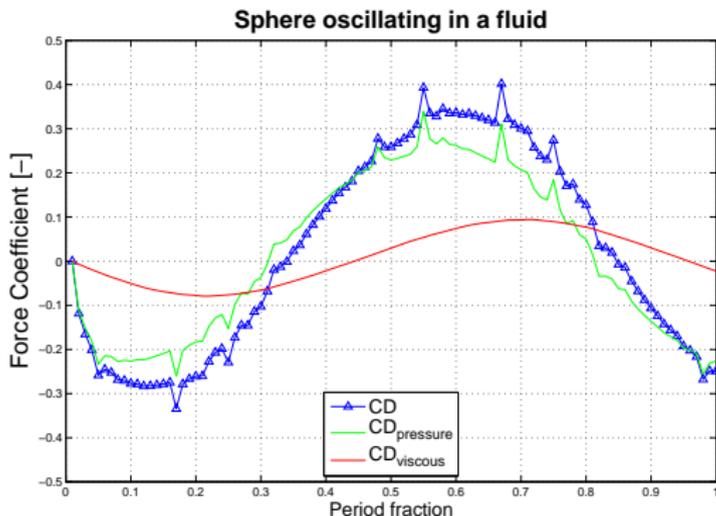
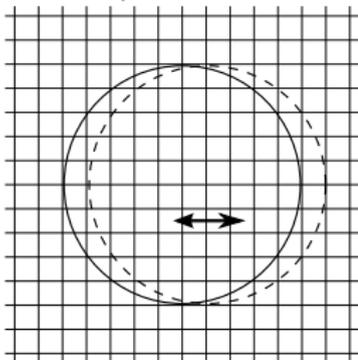
$$F_i = \int_{IB} \left(-p\delta_{ij} - \mu \left[\frac{\partial u_i}{\partial x_j} + \frac{\partial u_j}{\partial x_i} \right] \right) n_j dS$$

- Pressure:
Quadratic extrapolation from auxiliary points
- Viscous Terms:
Velocity gradients from least square fit of Taylor series



- Spurious pressure oscillation in simulations of moving bodies

$$\Delta x/D = 0.1,$$
$$\Delta t/T = 0.01$$



OSCILLATION SCALING

$$2D \approx \frac{(\Delta x)^2}{(\Delta t)}$$
$$3D \approx \frac{(\Delta x)^3}{(\Delta t)}$$

MASS CONSERVATION LAW FOR IB SIMULATIONS

$$-\frac{\Delta V_{IB}}{\Delta t} + \int_{\sigma_{cv}} \vec{U}_f \cdot \vec{n} dA = \frac{\Delta V}{\Delta t} (q^{n+1} - q^n) + S_\sigma$$

$\frac{\Delta V}{\Delta t} (q^{n+1} - q^n)$ - changes in fluid volume around IB

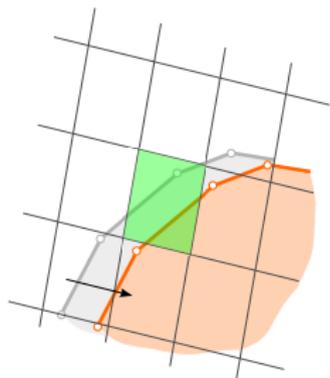
q^n - total number of solid cells at time n

ΔV - cell volume

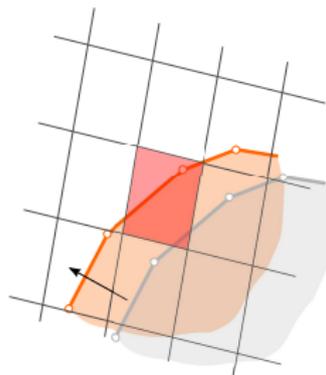
S_σ - "transpiration" error

- *RHS* represents the error in mass conservation
- Sudden changes in fluid volume around the body
- Experience high discontinuous variation in time

- Cells changing their behaviour:



fresh cells



dead cells

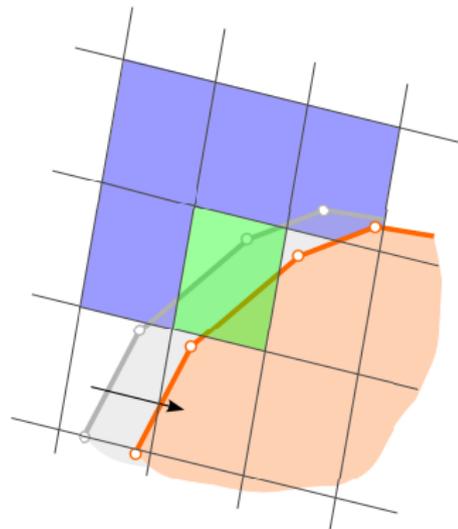
- Associated issues:
 - The “old” velocities and pressures in *fresh* and *dead* cells are not correct
 - Mass source error
 - Mirrored point change

PROPOSED IMPROVEMENTS

- *Fresh/dead* cell velocity and pressure interpolation
- Improving the mirroring interpolation
- Continuity equation modifications
 - Find the accurate cell areas and triangles in cells
 - Solve the continuity equation for the mirrored cells
 - Merge the mirrored cells with neighbouring fluid cells

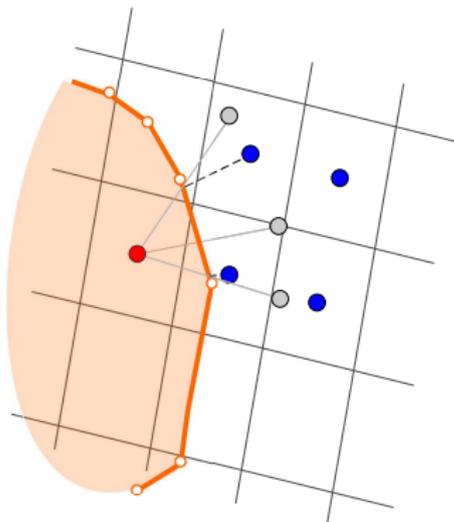
FRESH/DEAD CELL TREATMENT

- 1 Interpolate **velocity** to *fresh* cells from surrounding fluid cells
- 2 Interpolate **pressure** to *fresh* cells from surrounding fluid cells
- 3 Use the flow velocity and mirroring principle to estimate the velocity and pressure of mirrored points
- 4 Re-calculate the explicit mass flux in the vicinity of the body



MIRRORING INTERPOLATION COEFFICIENTS

- Use multiple surface points for setting the boundary condition
- Calculate weighted average of the coefficients
- Cells close to the surface are more important (large ϕ_k)

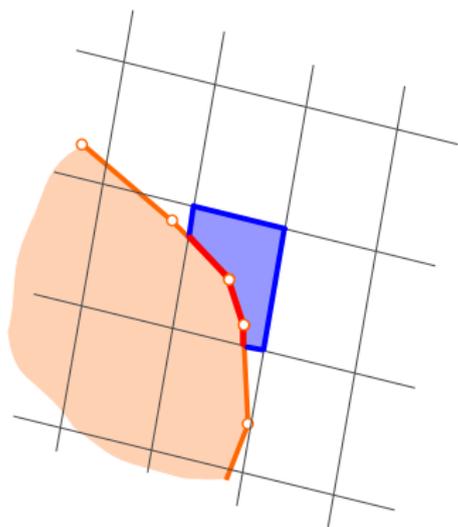


IMPROVED MIRRORING PRINCIPLE

$$\sum \phi_k u_{IB}^i = \sum \frac{1}{2} \phi_k (u_{IN}^i + \sum \beta_{m,k} u_m^i)$$

CONTINUITY EQUATION MODIFICATIONS

- Cut the fluid cells with the IB to get accurate flow areas and cell volumes
- Possible strategies:
 - Merge the mirrored cells with flow cells
 - Solve the continuity equation for mirrored cells

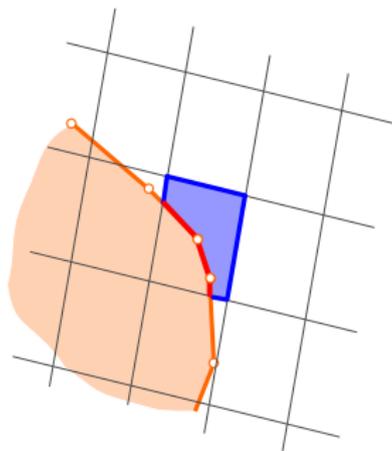


GRADIENT INTERPOLATION IN CUT CELLS

$$\frac{\delta\phi}{\delta x^i} = \sum (\phi_f a_f^{*i} + \phi_{IB}^i a_{IB}^{*i})$$

SOLVE CONTINUITY IN MIRRORED CELLS

- Solve the continuity equation in mirrored cells
- Reduces mass error
- Flow between mirror cells needs special treatment
- Small cells may be inaccurate

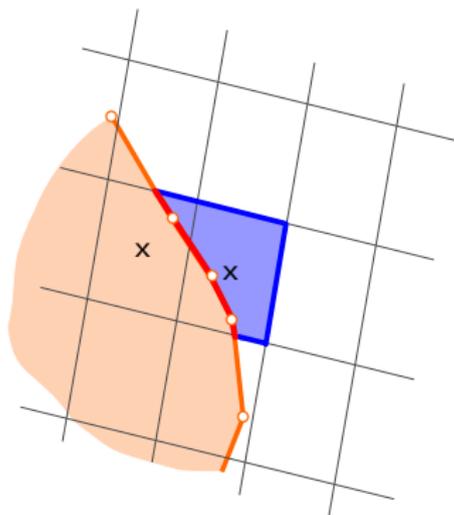


CONTINUITY EQUATION

$$\sum u_f^i a_f^{*i} + \sum u_{IB}^i a_{IB}^{*i} = \sum \left\langle \bar{u}_f^i + \hat{d}_f^{u^i} \left(\left[\frac{\delta \rho}{\delta x^i} \right]_f - \overline{\left[\frac{\delta \rho}{\delta x^i} \right]_f} \right) \right\rangle + \sum u_{IB}^i a_{IB}^{*i} = 0$$

CELL MERGING

- Merge to fluid cell with largest flow area
- Find the interpolation coefficients for the continuity in mirrored cell
- Add the contribution of the body motion
- Input the coefficients to the continuity equation for merged cell

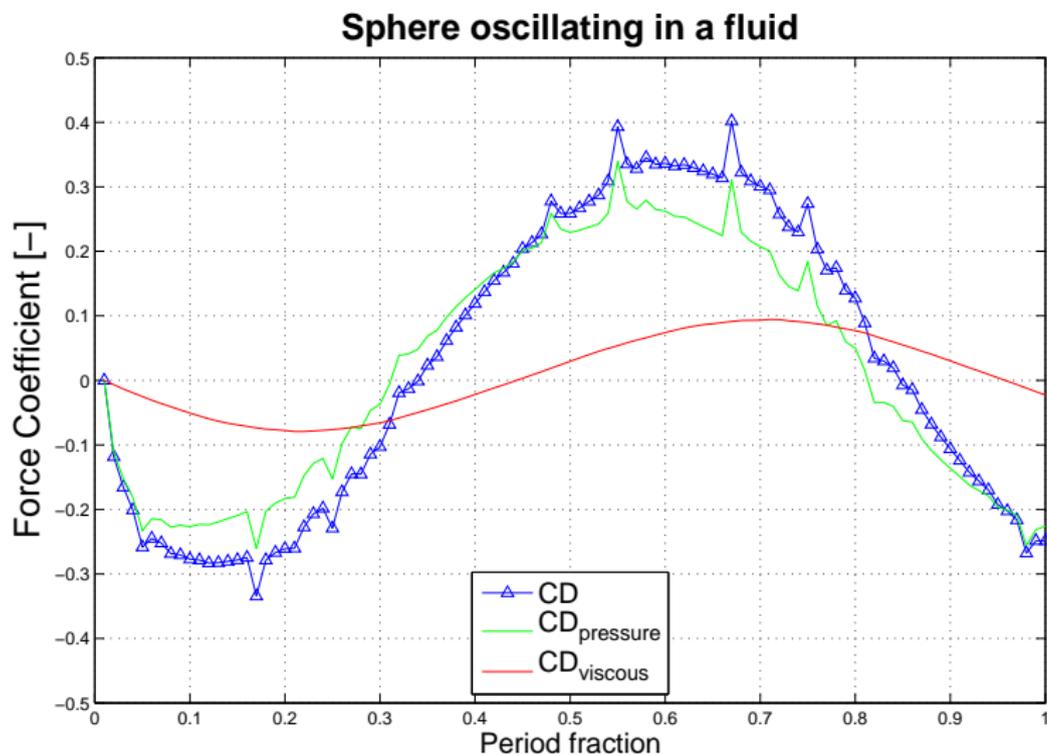


CONTINUITY EQUATION FOR MERGED CELL

$$\left(\sum u_f^i a_f^{*i} + \sum u_{IB}^i a_{IB}^{*i}\right)_{fluid} + \left(\sum u_f^i a_f^{*i} + \sum u_{IB}^i a_{IB}^{*i}\right)_{mirrored} = 0$$

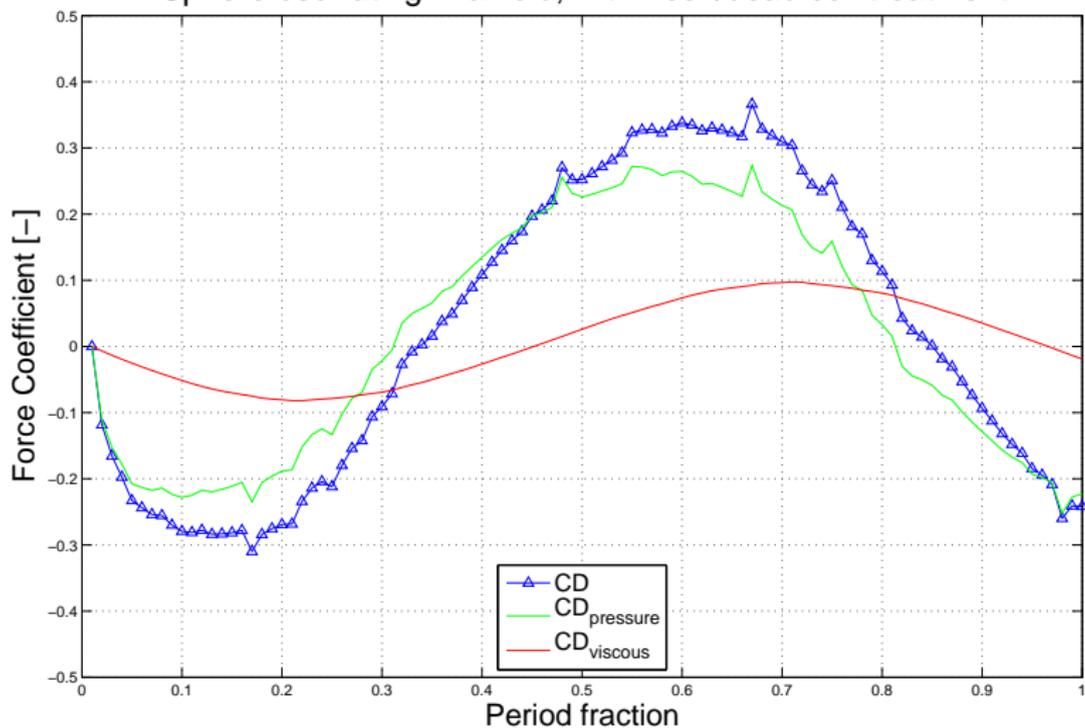
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OSCILLATING SPHERE ORIGINAL APPROACH

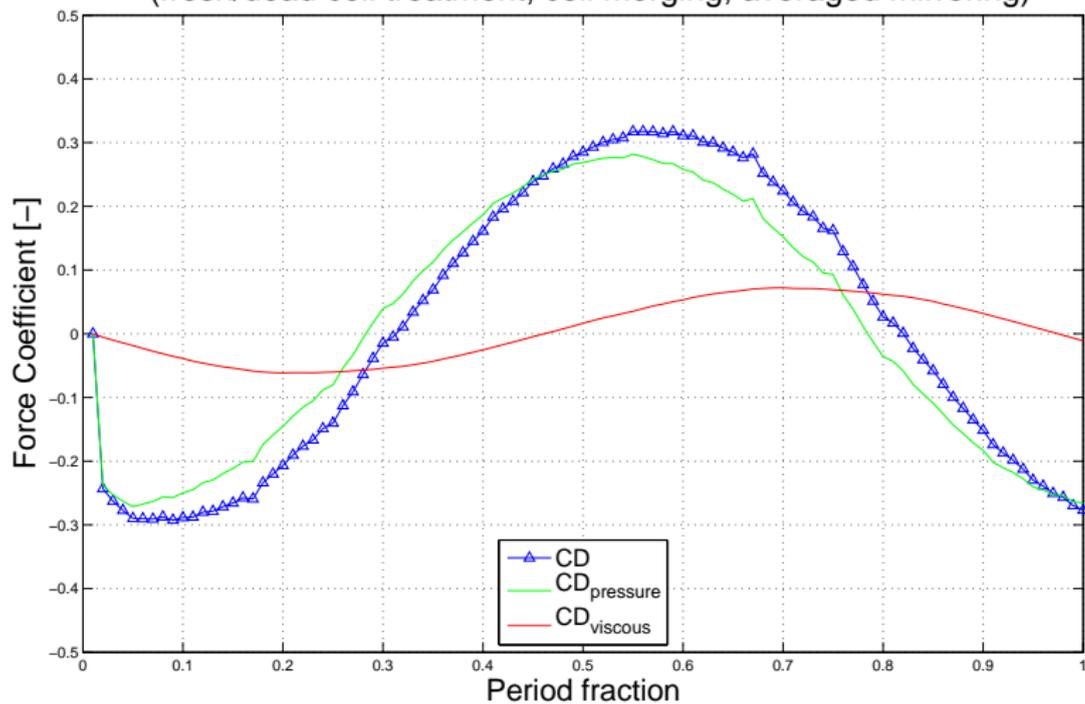


OSCILLATING SPHERE WITH FRESH/DEAD CELL TREATMENT

Sphere oscillating in a fluid, with fresh/dead cell treatment

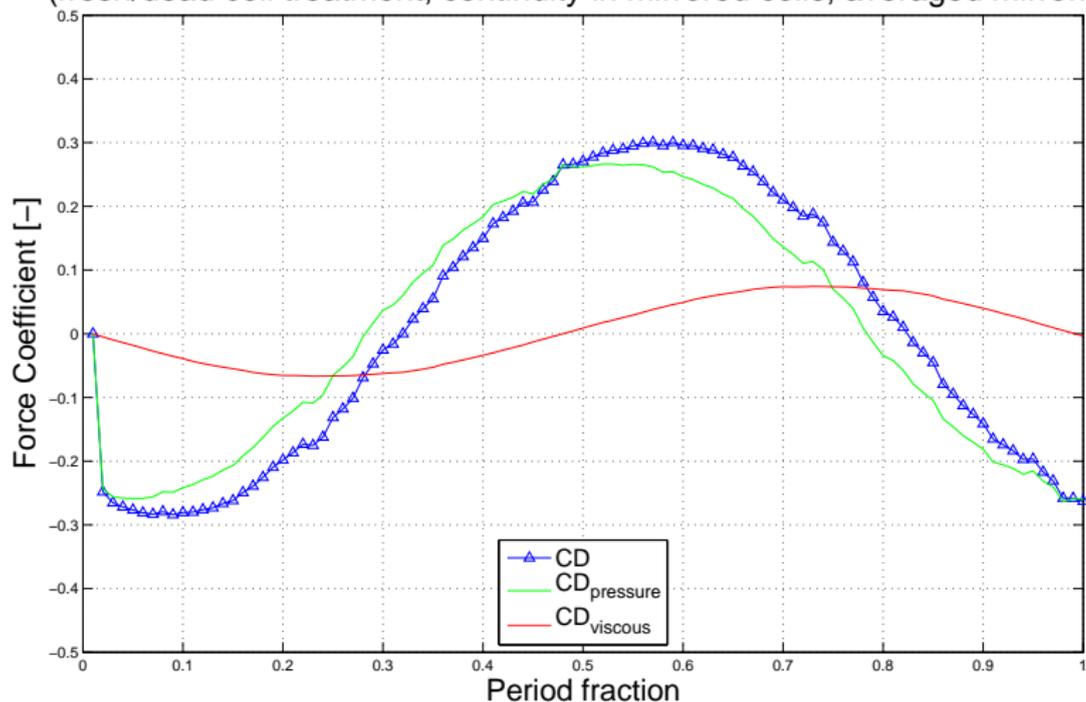


Sphere oscillating in a fluid,
(fresh/dead cell treatment, cell merging, averaged mirroring)



CONTINUITY IN MIRRORED CELLS

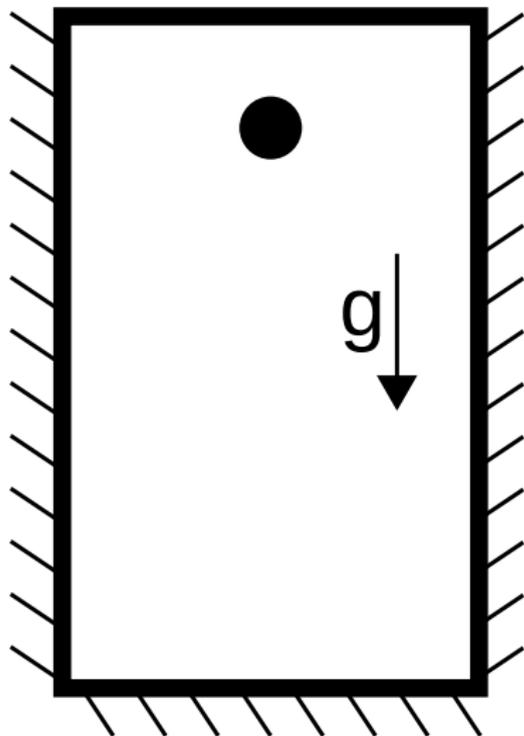
Sphere oscillating in a fluid,
(fresh/dead cell treatment, continuity in mirrored cells, averaged mirroring)



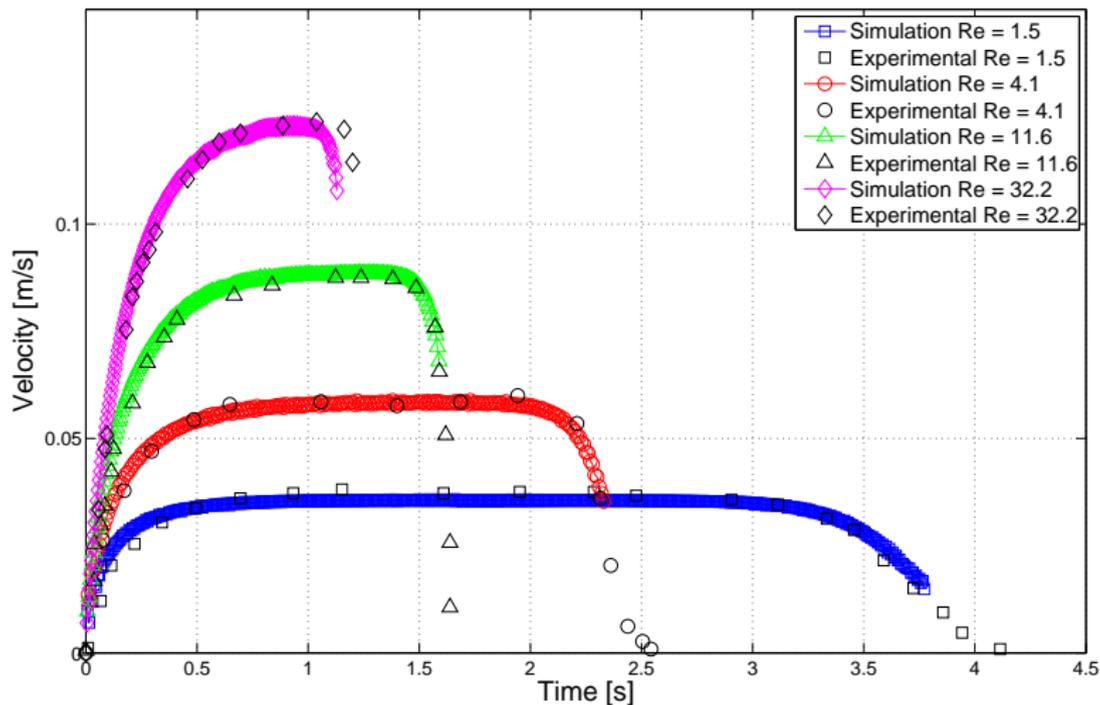
SPHERE SETTLING UNDER GRAVITY IN A TANK

- Experimental setup:
Ten Cate, 2002
- $D/\Delta x = 8$
- 4 cases considered
(adjustment of fluid density
and viscosity):

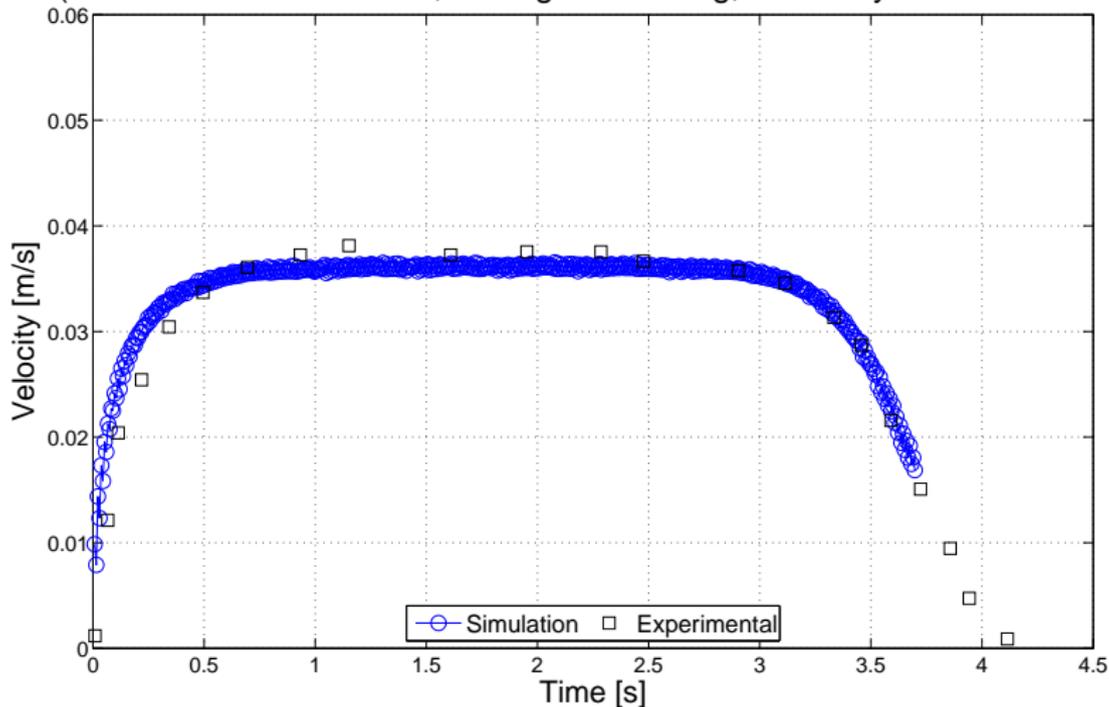
Case	u_t	Re_T
1	0.038	1.5
2	0.060	4.1
3	0.091	11.6
4	0.128	31.9



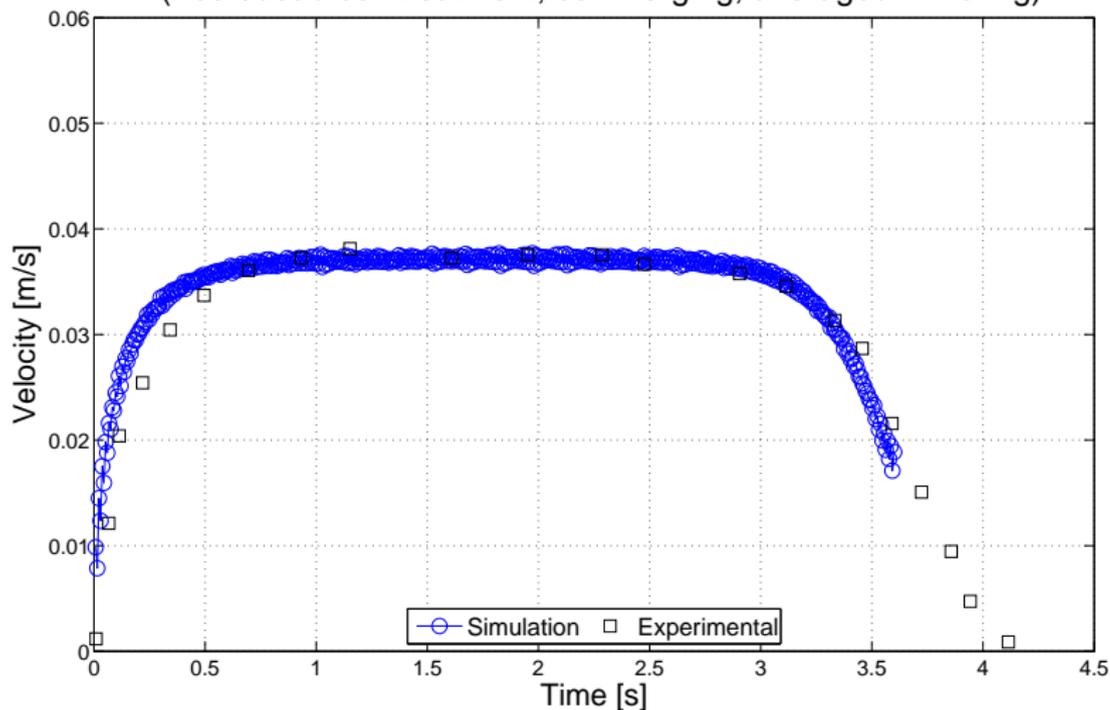
Sphere sedimenting in a tank
(fresh/dead cell treatment)



Sphere settling in a tank – Case: 1
(fresh/dead cell treatment, averaged mirroring, continuity in mirrored cells)



Sphere settling in a tank – Case: 1
(fresh/dead cell treatment, cell merging, averaged mirroring)

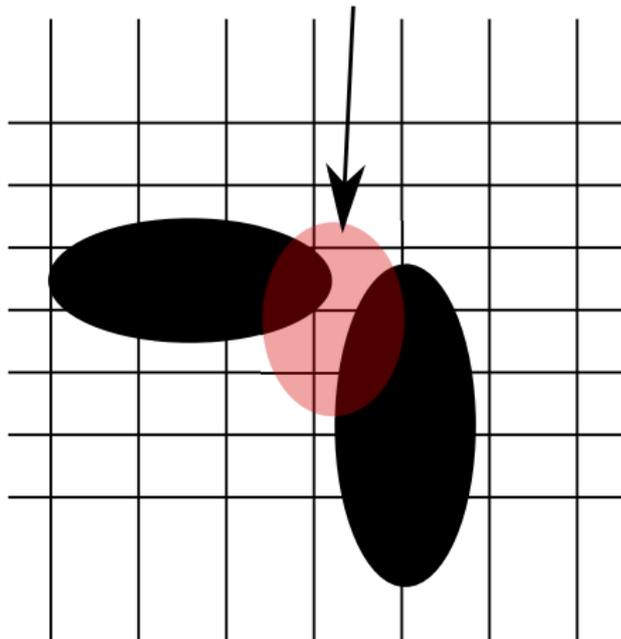


- Decreasing the oscillations:
 - Interpolation of flow between mirrored cells
 - Fresh/dead cell treatment
 - Mirroring technique
- Functionality of the method:
 - Force calculation improvement
 - Multiple particles
 - Particle-wall, particle-particle collisions

When 2 particles come close there are complications:

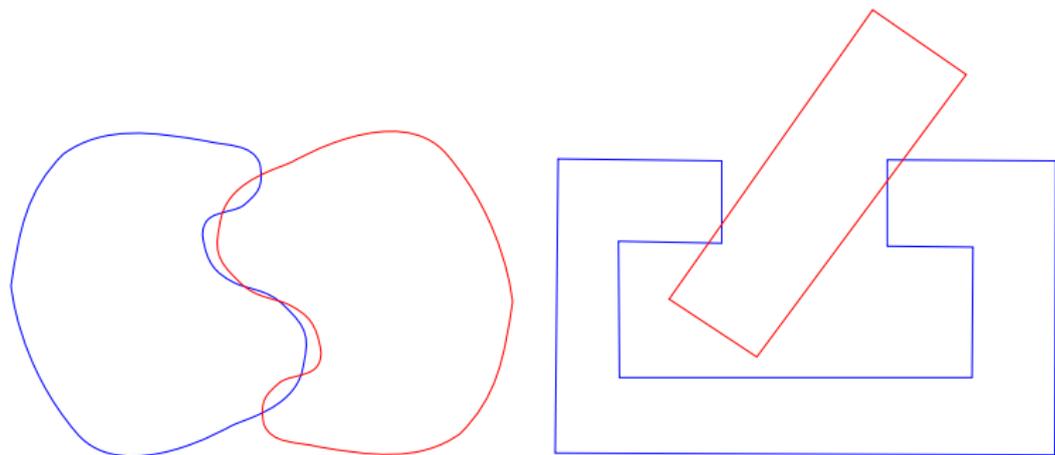
- 1 The fluid between the particles cannot be resolved.
- 2 The force from the fluid on the particles cannot be resolved.
- 3 The particles may collide.

how to treat the fluid cells?



Difficulty to describe collisions of particles with arbitrary shape:

- No canonical centre or contact direction.
- May have multiple contact areas.
- May be that a single contact point does not describe the contact, for example can have no net force, but a torque.
- During contact, the particle no longer has a closed surface with the fluid.



(a) No obvious contact position and direction

(b) Multiple contact patches cannot be seen as one

FIGURE : Two dimensional representations of contacts that have not got a simple parameterisation

PROPOSED DISCRETISATION SCHEME

- Breakdown overlap of particles into simple pieces
- Each piece bounded by only two triangles (one from each body)
- Each piece easily parameterised
 - Total volume
 - Centre of volume
 - Contact area
 - Contact direction
 - Effective curvature
- Easy to recombine to produce complex contact behaviour
- Closed surface for pressure re-obtained by using an additional internal pressure, calculated by smoothing the external pressure.

DISCRETISATION SCHEME CONTINUED

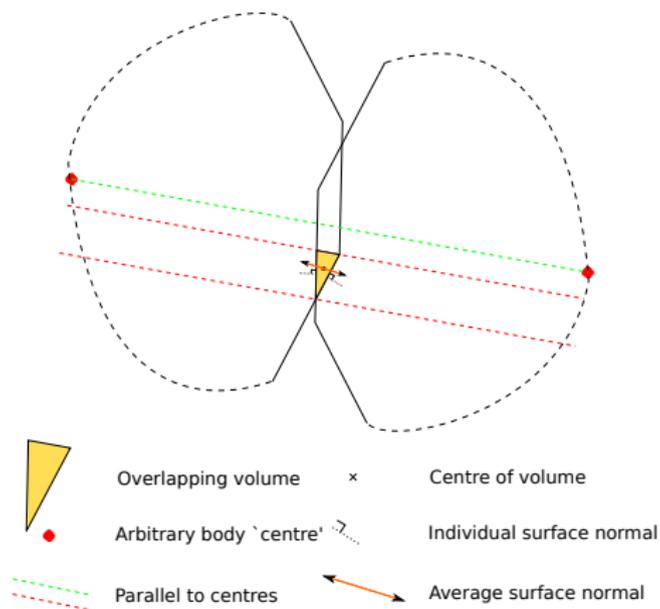


FIGURE : Decomposing of contact overlap into sections bounded by only two triangles

CURVATURE ESTIMATION

The curvature for each triangle is calculated in a Lagrangian framework:

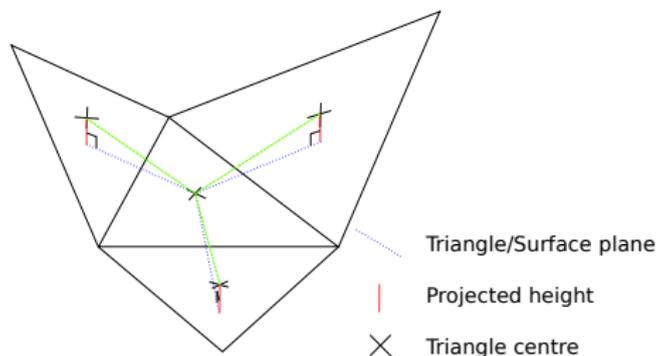


FIGURE : Decomposing of neighbouring triangle cell centres in in and out of plane components, in order to estimate curvature.

Curvature is fitted by comparing the in-triangle plane and out-of-plane components of the relative position of adjacent triangles. The in-triangle plane can be considered as is or fitted to account for skewness in the surrounding triangles.

And overall 'effective' curvature ($C_{\text{effective}}$) for the contact volume is considered by combining the curvatures of the two triangles that make it (C_A and C_B). This is done in the usual way.

$$C_{\text{effective}} = \frac{1}{\frac{1}{C_A} + \frac{1}{C_B}} \quad (1)$$

FLOW THROUGH PARTICLE ARRAY

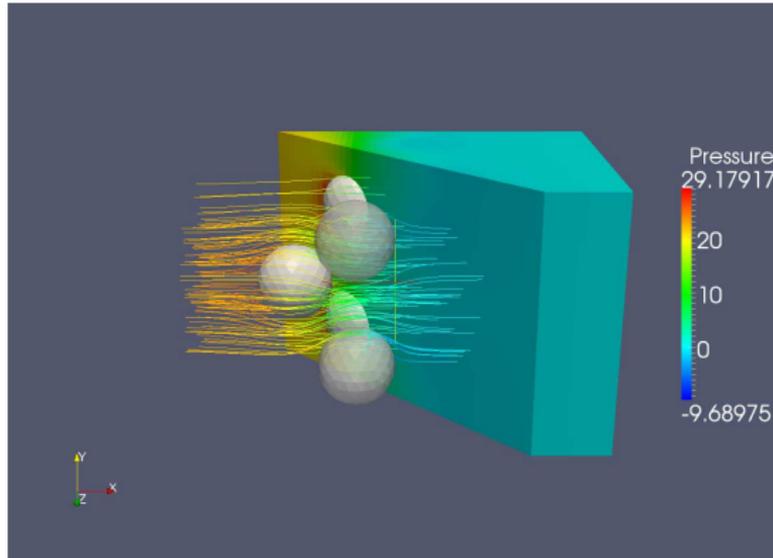


FIGURE : Flow past an array of 5 spheres

FLOW THROUGH PARTICLE ARRAY

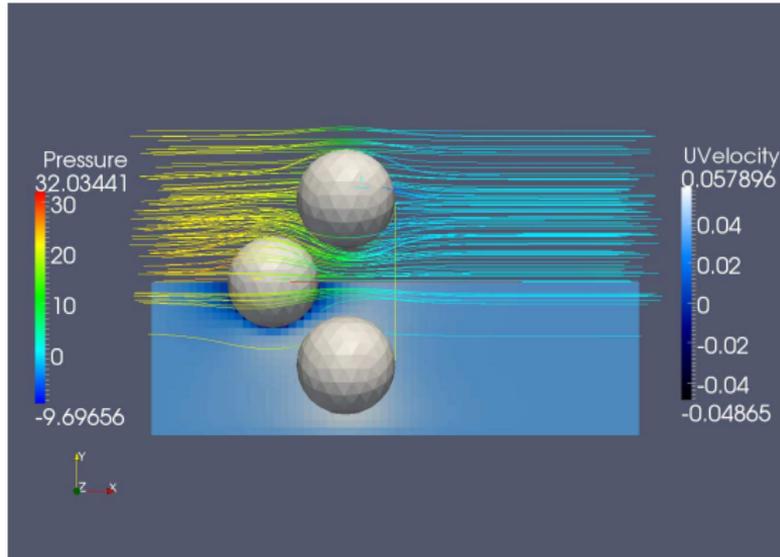
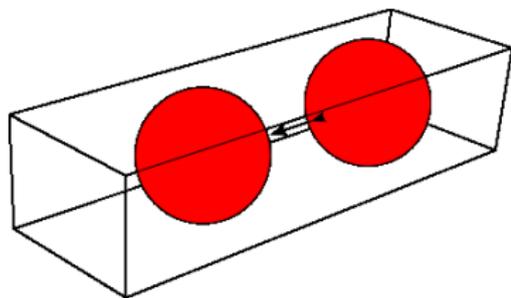
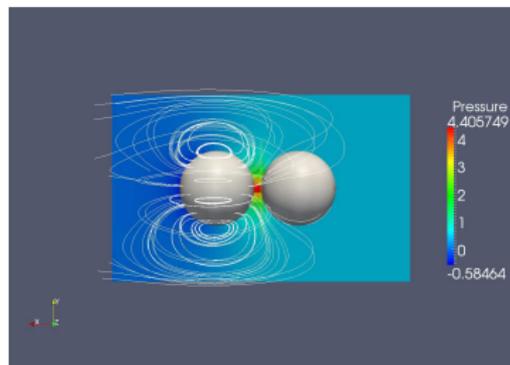


FIGURE : Flow past an array of 5 spheres

LUBRICATION FORCE SETUP



(a) Setup



(b) Flow around particles

FIGURE : Setup and flow field used to determine the lubrication force between two particles

LUBRICATION FORCE RESULT

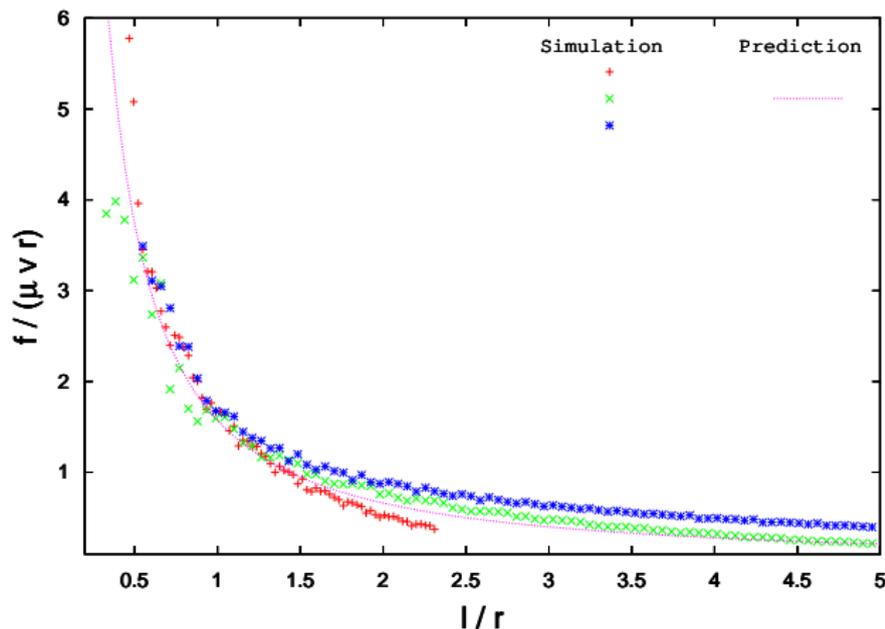
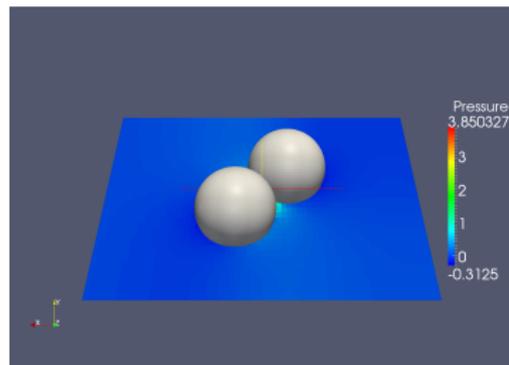


FIGURE : A plot of the non-dimensionalised lubrication force along with the proposed law, assuming low Reynolds number

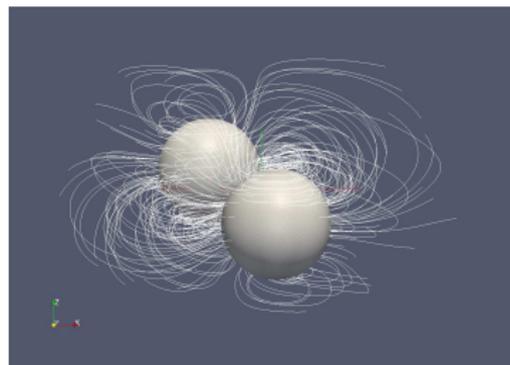
Non-dimensional lubrication force prediction.

$$\frac{F}{\mu \cdot v \cdot r} = \frac{\pi}{2} \times \left(\frac{r}{l}\right)^{1.25}$$
$$F = \frac{\pi \cdot \mu \cdot v \cdot r}{2} \times \left(\frac{r}{l}\right)^{1.25}$$

COLLIDING PARTICLE



(a) Interstitial pressure



(b) Streamlines of the fluid phase

FIGURE : Flow field around two obliquely colliding spheres

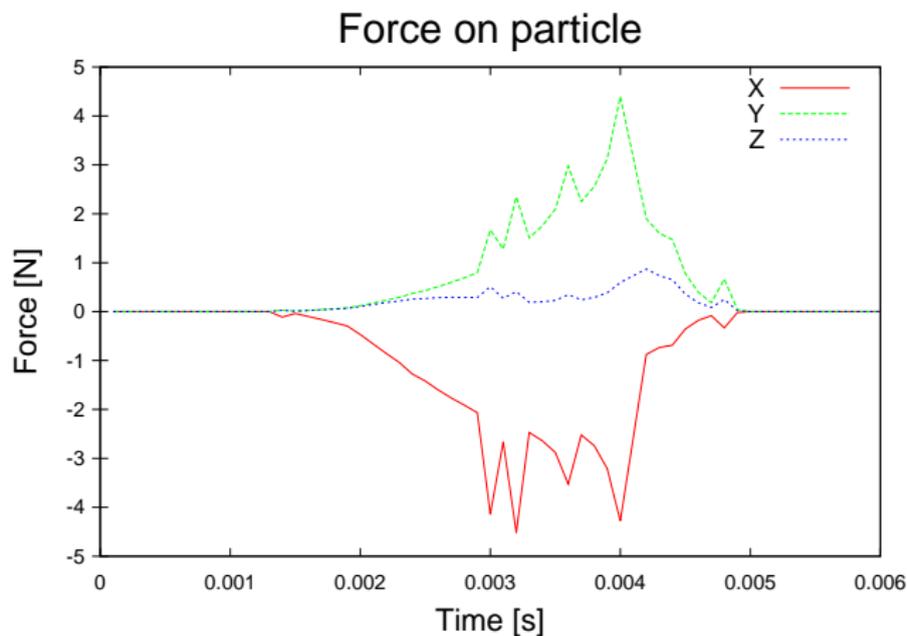
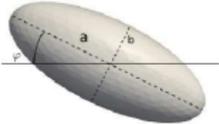
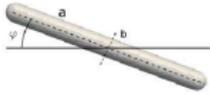


FIGURE : A plot of the components of collision forces between the particles

SOME EXAMPLES

- Disc falling in a fluid
- Disc falling in a fluid
- Disc falling in a fluid
- Collision of two particles
- Interacting particles
- Comparison of shape on settling
- Collision of two particles
- Interaction of bubble with particle
- Interaction of disc with free surface

PARTICLE SHAPES

shape	sphericity	proportions	size
sphere	1		$d = 200 \mu\text{m}$
			
ellipsoid	0.88	$\frac{a}{b} = \frac{5}{2}$	$a = 368 \mu\text{m}$ $b = 147 \mu\text{m}$
			
fiber	0.70	$\frac{a}{b} = 5$	$a = 510 \mu\text{m}$ $b = 102 \mu\text{m}$
			
disc	0.88	$\frac{a}{b} = 5$	$a = 350 \mu\text{m}$ $b = 70 \mu\text{m}$
			

FORCES AND TORQUES ON A PARTICLE

DRAG FORCE

$$F_d = C_D(\dots) \frac{1}{2} \rho_g \frac{\pi}{4} d_p^2 (\tilde{\mathbf{v}}_f - \mathbf{v}_p)^2$$

LIFT FORCE

$$F_l = C_L(\dots) \frac{1}{2} \rho_g \frac{\pi}{4} d_p^2 (\tilde{\mathbf{v}}_f - \mathbf{v}_p)^2$$

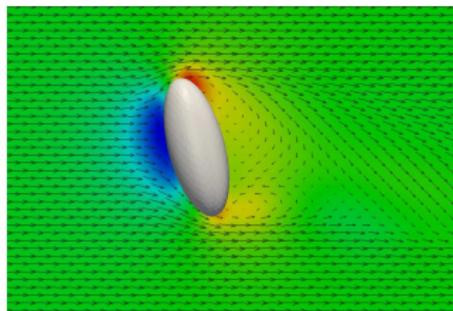
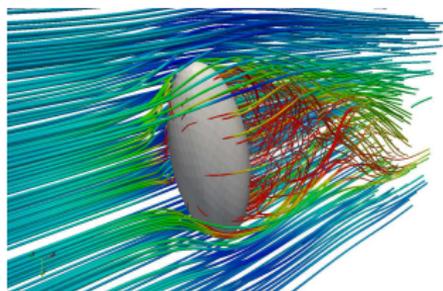
AERODYNAMIC TORQUE

$$T_{aero} = C_T(\dots) \frac{1}{2} \rho_g \frac{\pi}{8} d_p^3 (\tilde{\mathbf{v}}_f - \mathbf{v}_p)^2$$

ROTATIONAL TORQUE

$$T_{rot} = C_R(\dots) \frac{\rho}{2} \left(\frac{d_p}{2} \right)^5 |\omega_p| \omega_p$$

RESULTS: DNS SIMULATIONS



$$C_D(\varphi) = C_{D,\varphi=0^\circ} + (C_{D,\varphi=90^\circ} - C_{D,\varphi=0^\circ}) \sin^{a_0} \varphi$$

$$C_{D,\varphi=0^\circ} = \frac{a_1}{Re^{a_2}} + \frac{a_3}{Re^{a_4}}$$

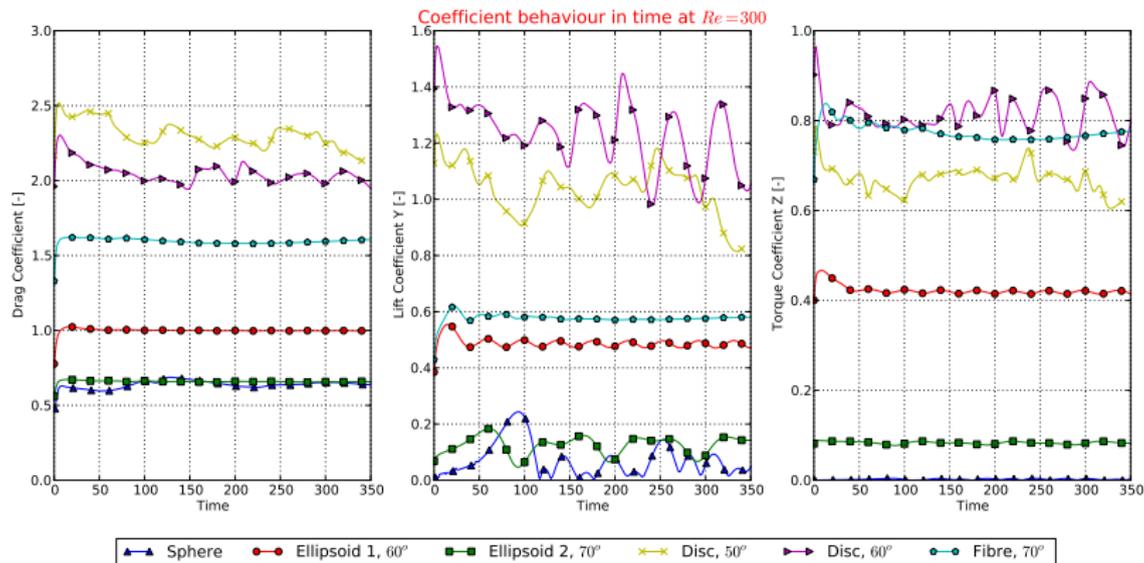
$$C_{D,\varphi=90^\circ} = \frac{a_5}{Re^{a_6}} + \frac{a_7}{Re^{a_8}}$$

$$C_L = \left(\frac{b_1}{Re^{b_2}} + \frac{b_3}{Re^{b_4}} \right) \sin(\varphi)^{b_5+b_6 Re^{b_7}} \cos(\varphi)^{b_8+b_9 Re^{b_{10}}}$$

$$C_T = \left(\frac{c_1}{Re^{c_2}} + \frac{c_3}{Re^{c_4}} \right) \sin(\varphi)^{c_5+c_6 Re^{c_7}} \cos(\varphi)^{c_8+c_9 Re^{c_{10}}}$$

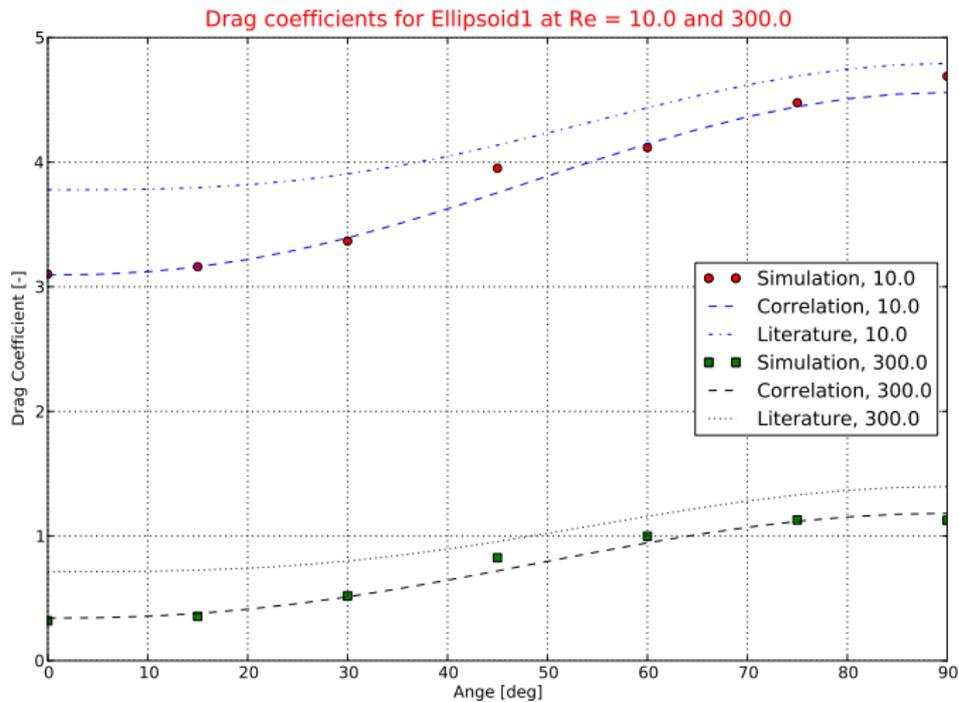
Zastawny et al. (2012) Int. J. Multiphase Flows 39, pp 227

RESULTS FROM DNS

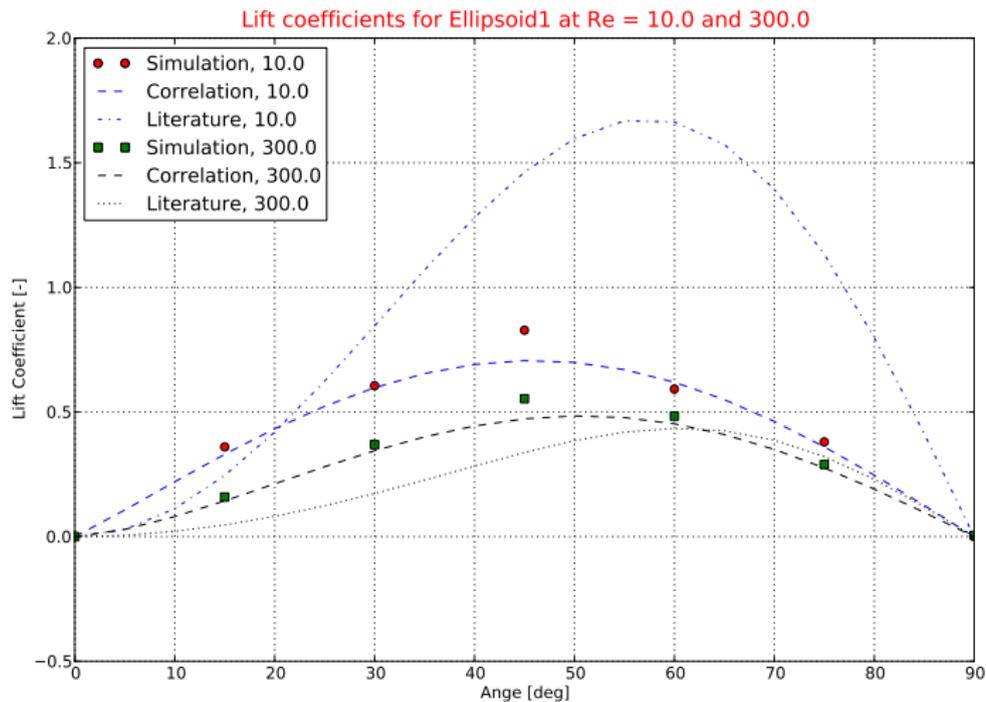


Zastawny et al. (2012) Int. J. Multiphase Flows 39, pp 227

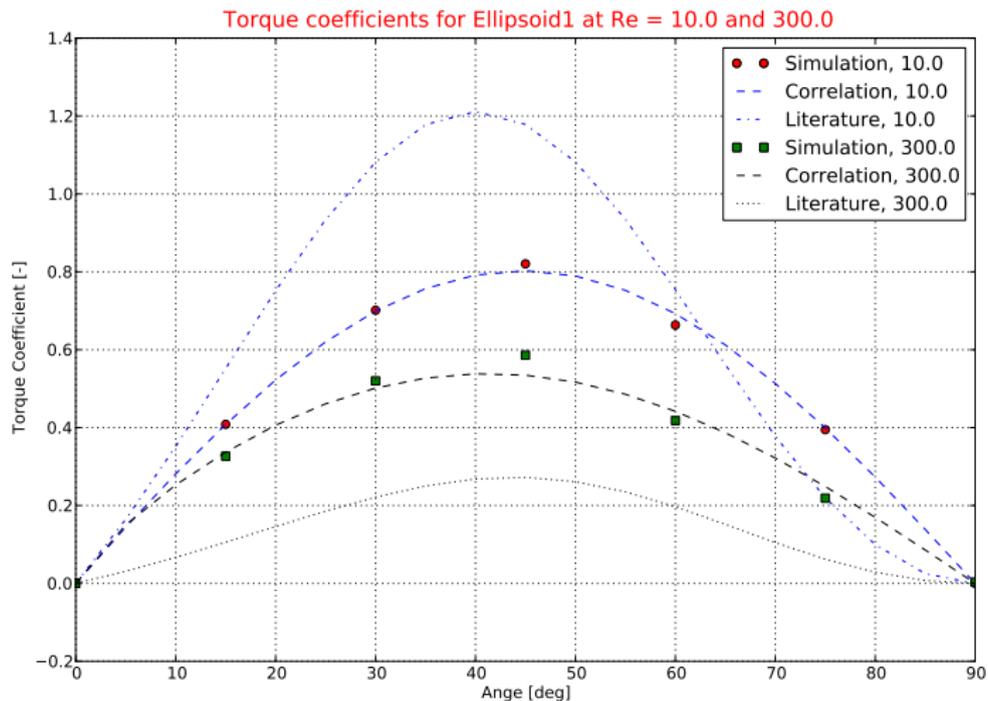
RESULTS FROM DNS



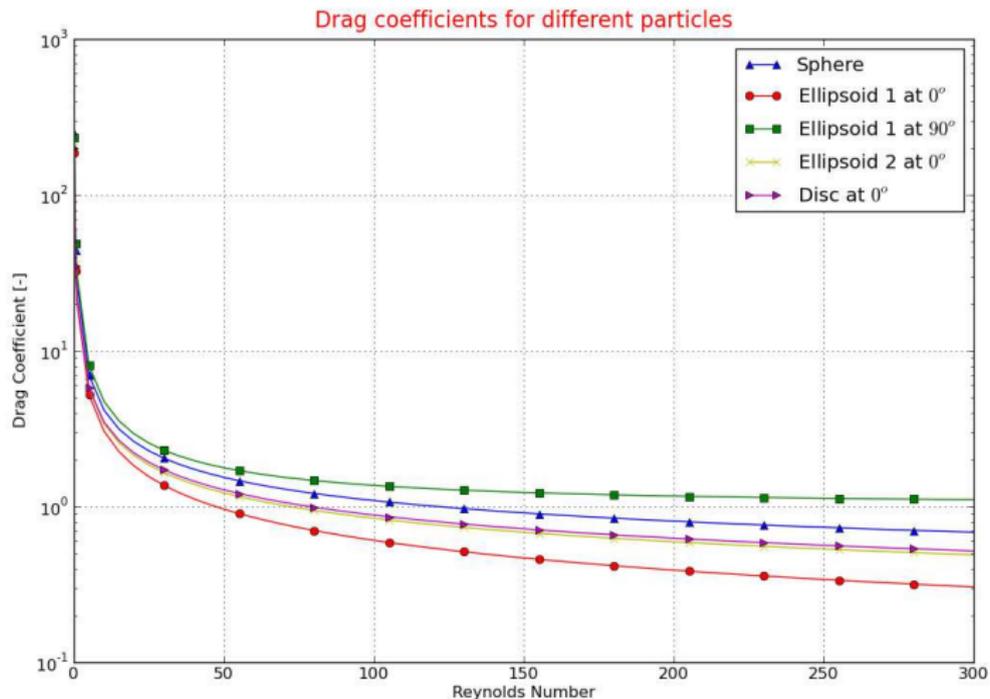
RESULTS FROM DNS

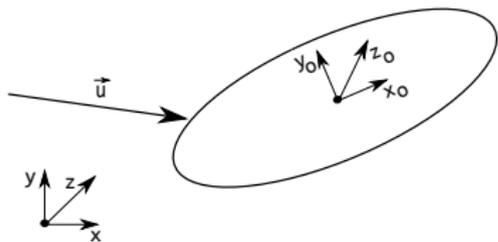


RESULTS FROM DNS

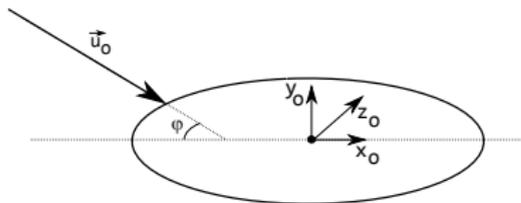


RESULTS FROM DNS





world space



body space

$$\varphi = \left| \arctan \left(\frac{u_{o,sh}}{u_{o,ln}} \right) \right|$$

$$F_{o,x} = \frac{1}{2} \cdot \rho \cdot A_{eq} \cdot C_D(\varphi, Re) \cdot |\mathbf{u}_o| u_{o,x} + F_L \cdot \sin \varphi \cdot \text{sign}(-u_{o,x})$$

$$F_{o,y} = \frac{1}{2} \cdot \rho \cdot A_{eq} \cdot C_D(\varphi, Re) \cdot |\mathbf{u}_o| u_{o,y} + F_L \cdot \cos \varphi \cdot \frac{u_{o,y}}{\sqrt{u_{o,y}^2 + u_{o,z}^2}}$$

$$F_{o,z} = \frac{1}{2} \cdot \rho \cdot A_{eq} \cdot C_D(\varphi, Re) \cdot |\mathbf{u}_o| u_{o,z} + F_L \cdot \cos \varphi \cdot \frac{u_{o,z}}{\sqrt{u_{o,y}^2 + u_{o,z}^2}}$$

Example Zhao and van Wachem, Acta Mechanica 224, 2013

- Discussion of Immersed Boundary Methods
- Shortcomings/treatments in IBM
- Particle-Particle interactions in IBM
- Deriving force/torque model from IBM